

1 **Atypical beta power fluctuation while listening to an isochronous sequence in dyslexia**

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29

30 **Highlights**

- 31 • Adults with dyslexia and matched controls listened to isochronous tone sequences.
- 32 • Dyslexia was associated with an atypical phase of beta (~20 Hz) power fluctuation.
- 33 • Atypical beta power fluctuation might reflect deficits in tracking auditory rhythm.

34

35 **Abstract**

36 *Objective*

37 Developmental dyslexia is a reading disorder that features difficulties in perceiving and tracking
38 rhythmic regularities in auditory streams, such as speech and music. Studies on typical healthy
39 participants have shown that power fluctuations of neural oscillations in beta band (15-25 Hz),
40 which are likely related to predictive timing and attentional processes, reflect an essential
41 mechanism for tracking rhythm or entrainment. Here we investigate whether adults with dyslexia
42 have atypical beta power fluctuation.

43

44 *Methods*

45 The electroencephalographic activities of individuals with dyslexia (n = 13) and typical control
46 participants (n = 13) were measured while they passively listened to an isochronous tone
47 sequence (2 Hz presentation rate). The time-frequency neural activities generated from auditory
48 cortices were analyzed.

49

50 *Results*

51 The phase of beta power fluctuation at the 2 Hz stimulus presentation rate differed and appeared
52 opposite between individuals with dyslexia and controls.

53

54 *Conclusions*

55 Atypical beta power fluctuation might reflect deficits in perceiving and tracking auditory rhythm
56 in dyslexia.

57

58 *Significance*

59 These findings extend our understanding of atypical neural activities for tracking rhythm in
60 dyslexia and could inspire novel methods to objectively measure the benefits of training, and
61 predict potential benefit of auditory rhythmic rehabilitation programs on an individual basis.

62

63

64 **Keywords:** Dyslexia, Electroencephalography (EEG), Beta oscillation, Auditory perception,
65 Entrainment.

66

67 **Abbreviations:** electroencephalography (EEG), event-related potential (ERP), independent
68 component analysis (ICA), standard deviation (SD).

69

70

71 **Introduction**

72 Developmental dyslexia is a common reading disorder with a prevalence rate of around 5
73 to 10% (Siegel, 2006), featuring impairments in phonological awareness, such as difficulties in
74 identifying rhyming words or syllabic stress patterns in speech (Goswami et al., 2013). Beyond
75 deficits in speech perception, this impairment is also associated with deficits of auditory
76 processing of rhythmic temporal regularity (Goswami, 2011, 2015, 2019), including detecting
77 amplitude envelope onset, perceiving and producing rhythm, and extracting auditory rhythmic
78 regularity (Flaugnacco et al., 2014; Huss et al., 2011; Leong et al., 2011; Leong and Goswami,
79 2014). The association between these two domains of auditory processing are also observed
80 among typically-developing children: rhythm perception and the ability to synchronize to a beat
81 are associated with phonological awareness, verbal short-term memory, rapid naming, and
82 morphosyntactic accuracy in speech production (e.g., Woodruff Carr et al., 2014). Despite this
83 evidence, we know little about the neural processing that underlies the rhythmic deficits in
84 dyslexia, the focus of the present paper.

85 Neural oscillations have been proposed as an essential mechanism for tracking rhythm
86 (Haegens and Zion Golumbic, 2018; Trainor et al., 2018). The power fluctuations of high-
87 frequency oscillations (beta band: 15–25 Hz) entrain to rhythmic regularity in sound streams.
88 When participants listen to an isochronous tone sequence, the beta band power from auditory
89 cortex decreases immediately following the onset of a tone, and then rebounds anticipatorily
90 according to the onset time of the upcoming tone (Cirelli et al., 2014; Fujioka et al., 2012),
91 consistent with a mechanism for predicting the onset time of the next expected tone. This
92 entrainment activity can be modulated by hierarchical rhythmic structure or disrupted by a
93 random sequence (Fujioka et al., 2009; 2015; Iversen et al., 2009; Snyder and Large, 2005), and

94 it is associated with auditory prediction, attentional processing and perceptual performance
95 (Chang et al., 2018, 2019; Morillon and Baillet, 2017). Atypical beta power entrainment
96 activities have been observed in populations featuring deficits in rhythm perception and tracking,
97 such as patients with Parkinson’s disease (te Woerd et al., 2017, 2018) and children with
98 stuttering (Etchell et al., 2016). However, it is unknown whether atypical beta power entrainment
99 to auditory rhythmicity is associated with dyslexia.

100 In the present study, we measured the electroencephalographic (EEG) activities of
101 individuals with dyslexia while they passively listened to an isochronous tone sequence. We
102 hypothesized that the beta power fluctuation generated from auditory cortex is different between
103 individuals with dyslexia and typical controls.

104

105 **Methods**

106 *Participants*

107 Thirteen adults with developmental dyslexia (seven women, ten right-handed; mean age
108 = 23.2 years, SD = 2.95 years) and 13 matched controls (seven women, seven right-handed,
109 mean age = 22.5 years, SD = 2.07) participated in the current experiment. Although handedness
110 was not perfectly matched in the current study, the higher proportion of non-right-handers
111 appears to be a feature of dyslexia (e.g., Eglinton and Annett, 1994). All participants reported
112 French as their native language, with one dyslexic participant reporting bilingualism with
113 English. None reported auditory deficits. Education levels did not differ between the Dyslexic
114 group (mean = 14.92 years; SD = 1.55) and the Control group (mean = 15.31 years, SD = 0.95),
115 $p = .45$. Musical background, as measured by years of instrumental instruction, also did not

116 differ between the Dyslexic group (mean = 2.00 years; SD = 2.16) and the Control group (mean
117 = 1.69 years, SD = 2.13), $p = 0.72$.

118 Participants with dyslexia were part of a larger research project investigating dyslexia at
119 the university level (Abadie and Bedoin, 2016; see Canette et al., 2020, Fiveash et al., 2020, for
120 more information). As detailed in Table S2, they completed a set of language and
121 neuropsychological tests, confirming the persistence of dyslexia for each participant. All
122 participants with dyslexia reported having seen a speech therapist for a dyslexia diagnosis and
123 for training designed to reduce reading difficulties for at least two years (and maximum 5 years)
124 during childhood, which in France is generally defined as between 8 and 13 years old. They
125 mainly have phonological difficulties (i.e., phonological or mixed forms of dyslexia, which are
126 the most frequently observed forms of this neurodevelopmental pathology). Note that all
127 participants with dyslexia had scores in the normal range for nonverbal intelligence (as measured
128 by Raven's Matrices) and they also performed in the normal range for reading comprehension
129 (average z-score placed them above the mean = 1.91, SD = 0.60). None of the participants
130 reported psychiatric or neurological diagnoses or attention disorder with/without hyperactivity.
131 On the other hand, none of the controls reported a history of spoken or written language
132 disorders. In particular we confirmed that, while at school, they did not have any difficulties in
133 language understanding or production or learning to read, and none had been followed up by a
134 speech therapist.

135 Written informed consent based on the French ethics procedure approval Committee
136 (CPP Sud-Est II, 2007-009-3) was obtained from all participants prior to participating in the
137 experiment, which was conducted in accordance with the guidelines of the Declaration of

138 Helsinki. Participants received a compensation of 12 Euros per hour for their participation in the
139 study.

140

141 *Stimulus*

142 During the EEG recording, participants passively listened for 5 minutes to an isochronous
143 sequence of piano tones with an inter-onset interval of 500 ms, which is in the tempo range that
144 gives rise to a strong sense of the beat (Drake et al., 2000; Merchant et al., 2015). The tone was
145 C4 (262 Hz), from the University of Iowa Musical Instrument Samples, and the amplitude
146 envelope of the piano tone was percussive with 10 ms rise times. Tones were truncated to be 200
147 ms in duration, and a linear decay to zero was applied over the entire excerpt to remove offset
148 artifact (Figure S3). For the behavioural post-test synchronization task, the same tone was
149 played with the same inter-onset interval for either 10 repetitions (training trial) or 40 repetitions
150 (experimental trials).

151

152 *Procedure*

153 To keep participants awake and still, they watched a silent black and white movie with
154 Charlie Chaplin while they listened passively to the 5-minute isochronous tone sequence (and
155 two other rhythmic patterns, not presented here) while EEG was continuously recorded¹. This
156 EEG recording was part of a longer experimental session and followed a priming experiment
157 with an active task (reported in Canette et al., 2020 and Fiveash et al., 2020). After the EEG
158 recording session, participants came back to the laboratory for a second testing session and

¹ It is a common approach to have participants watch a silent movie during a passive listening task to keep them awake and reduce eyeblinks or eye movements during EEG/MEG recordings. As the movie is not time-locked to the tone sequence and is not rhythmic, its influence on EEG analyses is negligible (e.g., Kong et al., 2014; Luo and Ding, 2020).

159 completed a set of behavioural tests on syntax processing and rhythm perception and production
160 based on the complex Beat Alignment Task (Einarson and Trainor, 2015; data presented in
161 Canette et al., 2020) and two rhythmic patterns (except for one dyslexic participant who did not
162 come back to this second session); these data were presented in Canette et al. (2020). In addition,
163 relevant for the present experiment, participants performed a production task where they were
164 required to tap along to the excerpts of the isochronous sequence used in the EEG session (i.e.,
165 inter-tone-onsets of 500 ms). Participants drummed with a stick on a drum pad (Roland, V-
166 Drums) to each tone. Both the passive listening and production parts were implemented with the
167 software Presentation (Neurobehavioural Systems), and stimuli were presented over headphones
168 (Pioneer, HDJ-500). During a training trial, they tapped to a sequence of 10 tones. Following
169 this, they completed two trials of 40 tones (i.e., 20 s duration) each.

170

171 *EEG recording and preprocessing*

172 The EEG signal was recorded with 95 Ag/AgCl active electrodes (actiCAP 96Ch
173 Standard-2, Brain Products GmbH). The signal was recorded with a BrainAmp amplifier at a
174 resolution of 16 bits, a sampling rate of 500 Hz, and with an analog low pass filter of 1000 Hz
175 and high pass filter of 0.016 Hz. The ground electrode was placed at position AFz, the reference
176 electrode on the tip of the nose, and an eye-movement monitoring electrode under the right eye
177 at position Iz. Electrode impedances were kept below 20 k Ω , which is a well acceptable
178 impedance levels for EEG recordings (e.g., Ferree et al., 2001; Luck, 2014). Continuous EEG
179 data were transformed to an average reference offline. The EEG data was further processed in
180 MATLAB with the FieldTrip toolbox (RRID: SCR_004849) (Oostenveld et al., 2011).

181 Independent component analysis (ICA) was used to remove artifact signals (Jung et al.,
182 2000). To speed up the ICA performance, the continuous recordings were downsampled to 250
183 Hz, filtered between 0.7 and 83 Hz and then segmented into time window from -3 to 303 s time-
184 locked to the first tone of the sequence. This window covered the entire stimulus sequence
185 length. We went back to the unfiltered data, projected it to ICA space and the ICs reflecting
186 artifact (identified by visual inspection, range of 2-13 ICs), including eye blinking, eye
187 movement, electrocardiogram, and powerline noise, were excluded, and then the data in the ICA
188 space was projected back to 95-channel space for all subsequent analyses.²

189

190 *Modeling dipole sources for auditory cortex*

191 In the present study, we focused on the responses generated from auditory cortex, as prior
192 studies have shown that auditory beta oscillations are related to temporal prediction and rhythmic
193 tracking (Chang et al., 2018, 2019; Cirelli et al., 2014; Fujioka et al., 2012, 2015). To achieve
194 this goal, we used a dipole model as a spatial filter to largely separate the activities of auditory
195 cortex from other sources, **following the studies cited above**, which is preferred to analyzing data
196 on selected surface electrodes, as each surface electrode reflects a mixture of activities from
197 many brain sources. The P1 ERP component (~60-90 ms) was used to localize bilateral auditory
198 cortices, with the dipole locations (but not orientation) constrained to be bilaterally symmetric.

² Although the electromagnetic field of the headphones was not masked, which might lead to some contamination of EEG recordings from sound waveforms, any potential headphone artifact should have had a negligible influence on our beta band findings because: (1) the observed beta power fluctuation shape was similar to those of previous studies (see *Power spectrum of beta power time series*); (2) we observed group differences (while a potential artefact would have equally affected recordings of each participant); and (3) this potential artifact was most likely attenuated by the ICA procedure. A potential artifact might have had more influence on early ERP analyses (reported in the *Supplementary Materials*), which showed somewhat atypical scalp topography in comparison with previous studies.

199 We used the multiple source probe scan algorithm and the four-shell ellipsoid model included in
200 the Brain Electrical Source Analysis (BESA, RRID: SCR_009530) software package. We chose
201 P1 because (1) it is primarily generated from primary auditory cortex (Godey et al., 2001), (2) it
202 is the dominant peak at fast presentation rates while the N1 peak is strongly reduced at fast rates
203 relevant to the current study (Näätänen and Picton, 1987), and (3) previous studies with similar
204 experimental designs also used P1 for localizing auditory cortex (e.g., Fujioka et al., 2012). The
205 mean locations (averaged across participants) of the fitted dipoles were [± 44.23 , -1.95 , 7.26]
206 (Talairach coordinates) with approximate mean orientations [0.2 , 0.5 , 0.8] (left) and [-0.2 , 0.6 ,
207 0.8] (right). These locations are close to bilateral primary auditory cortices with orientations
208 toward the mid-frontal surface area, consistent with typical auditory evoked potentials. The mean
209 residual variances of the source fittings were 7.9% (range 3.4 to 16.3%) for the Control group
210 and 7.0% (range 2.4 to 15.4%) for the Dyslexia group, and the residual variances were not
211 different between groups ($t(24) = 0.67$, $p = 0.509$). Finally, the unfiltered continuous 95-channel
212 EEG was projected into source-space EEG via the dipole model for further time-frequency
213 analyses.

214 Note that it is important that we perform the analyses at dipole locations, as the MEG
215 study of Fujioka et al. (2012) reported that the beta power generated in motor regions fluctuated
216 at the opposite phase of the beta power in auditory cortex. As the spatial resolution of EEG is
217 less precise than MEG, these two signals are likely to be mixed and potentially cancel each other
218 in EEG analyzed from the surface channels.

219

220 *Time-frequency analyses*

221 The unfiltered continuous source-space EEG data was segmented to include non-
222 overlapping epochs of 20 tones each. Each epoch was thus 11 s long, including 0.5 s prior to the
223 first tone and 0.5 s following the twentieth tone as buffer periods to avoid edge artifacts for the
224 time-frequency analysis. The first epoch at the beginning of each recording was excluded from
225 further analysis, as the rhythmic temporal regularity might not yet be perceived. Subsequently,
226 epochs were excluded that were greater than 150 μV to ensure artifacts were eliminated that were
227 not removed by ICA. The mean number of usable trials was 23.8 in the Control group and 26.7
228 in Dyslexia group; this was not significantly different between groups ($t(24) = 1.20, p = 0.244$).

229 We focused on the induced (non-phase-locked) power in beta band, following our
230 previous studies (e.g., Fujioka et al., 2012; Chang et al., 2016a, 2018, 2019; Cirelli et al., 2014).
231 For each participant, the unfiltered mean ERP waveform (averaged across trials) was subtracted
232 from each epoch to obtain induced waveforms (Fujioka et al., 2012; Cohen, 2014). We used a
233 short-time Fourier transformation with overlapped time windows (moving successively by one
234 sample) to perform the time-frequency transformation for 15-25 Hz (frequency bin size = 1 Hz).
235 The window size was fixed at 500 ms and a Hanning taper was applied. For each frequency bin,
236 the power was baseline corrected (percentage change) to the mean power for the 0-10 s window,
237 then the beta power was obtained by averaging the power across 15-25 Hz bins. To further
238 analyze the fluctuation of the beta power time series, we performed another Fourier
239 transformation with a Hanning taper for the beta power time series for each 10 s epoch (single-
240 trial), excluding the 0.5 s buffer periods at both ends.

241 Although some studies have defined the range of beta band to be as wide as 13-30 Hz, we
242 defined it as 15-25 Hz for several reasons. (1) It is consistent with our previous studies (e.g.,

243 Fujioka et al., 2012; Chang et al., 2019). (2) Some other studies have interpreted activities below
244 15 Hz as alpha band (e.g., Ahveninen et al., 2017) and above 25 Hz as low-gamma band (e.g.,
245 Giroud et al., 2020). Therefore, it is debatable whether to include these frequencies as beta band.
246 (3) Considering the imprecision of time-frequency analysis in terms of frequency resolution,
247 activities closer to 13 or 30 Hz will be more likely contaminated by activities below 13 or above
248 30 Hz, respectively, compared to frequencies between 15 and 25 Hz.

249 For completeness, we also analyzed event-related potentials (ERPs) (see *Supplementary*
250 *Materials*).

251

252 *Tapping production task*

253 We used circular statistics (Berens, 2009; Dalla Bella and Sowinski, 2015) to analyze the
254 production performance of the synchronization task for isochronous sequences, leading to two
255 measures related to the resulting vector R: its *angle*, representing synchronization accuracy and
256 its *length*, representing synchronization consistency (ranging from 0 to 1, with 1 representing
257 perfect consistency).

258

259 *Statistics*

260 We used a nonparametric cluster-based permutation test to analyze the EEG measure
261 difference between groups with the FieldTrip toolbox (Oostenveld et al., 2011). In short, this
262 procedure reduces the number of multiple comparisons by testing the statistical difference at the
263 level of time and/or frequency clusters instead of individual time and/or frequency points, and it
264 has been widely used for analyzing EEG and MEG data (see Maris and Oostenveld, 2007 for
265 more details). Specifically, first we performed a two-sample t-test between the two groups

266 (Dyslexia, Control) for each time or frequency sample as the initial scan for clustering. Second,
267 we grouped adjacent frequency (Figure 1B) or time (Figure S1A and S1C) samples reaching a
268 threshold of $p < 0.05$ in the initial scan into single clusters and summed the t-values of all
269 samples within each cluster as a cluster-level statistic. Third, we built a null distribution with
270 1000 random iterations. In each iteration, we pooled all 26 participants (13 in Dyslexia group
271 and 13 in Control group), randomly split participants into 2 equal-size groups, and performed the
272 same calculations as in the first two steps. The null distribution was composed by the summed t-
273 values of the largest suprathreshold cluster of each iteration, and the final p-value was obtained
274 by comparing the observed clustered summed t-value relative to the null distribution. In sum, if
275 there was no group difference, the cluster(s) of the observed data should resemble the random-
276 split data of the null distribution. The final p-value was corrected to two-tailed.

277 The circular statistics were computed in the Circular Statistics Toolbox for MATLAB
278 (Berens, 2009). Participant group differences for *R angle* and *length* were assessed with two-
279 tailed independent tests.

280 Note that the Watson-Williams test assumes the data to be distributed according to a von
281 Mises distribution, i.e., with concentration parameter (κ) equal or above 1. Therefore, we
282 examined whether our 2 Hz beta power fluctuation time series met this assumption. The κ
283 parameter was similar between compared datasets (difference range: 0.05-0.14), with only κ
284 parameters of the left and right auditory cortex of the Control group above 1. Although our data
285 did not fully satisfy the assumptions, the Watson-Williams test is considered robust against
286 deviations from these assumptions (Berens, 2009).

287

288 **Results**

289 *Power spectrum of beta power time series*

290 The beta power time series of left and right auditory cortex are visualized in Figure 1A.
291 The Control group showed typical beta power fluctuations in that the peaks occurred at the
292 approximate times of tone onsets (with anticipatory increase in power prior to tone onsets) and
293 troughs between tones. This pattern is similar to those observed in previous studies (e.g., Chang
294 et al., 2019; Fujioka et al., 2012, 2015). In contrast, the beta power fluctuations appear atypical
295 in the Dyslexia group in that troughs occurred at the approximate times of tone onsets and peaks
296 occurred between tones.

297 =====

298 Figure 1

299 =====

300 To examine the frequency characteristics of the beta power fluctuations, we frequency-
301 transformed the beta power time series into a power spectrum for each participant. The spectra of
302 beta power fluctuations (note that this is not the spectra of raw EEG waveform) are shown in
303 Figure 1B. The cluster-based permutation tests on left or right auditory cortex did not show any
304 significant differences in the power spectrum of beta power fluctuations between the Dyslexia
305 and Control groups (range of power fluctuations 1-5 Hz). There was also no interaction between
306 left/right auditory cortex and groups.

307 The frequency spectrum of beta power fluctuation (Figure 1B) did not show an obvious
308 peak at 2 Hz as expected, despite the appearance of a power fluctuation around the 2 Hz tone
309 onset rate in the averaged time domain waveforms (Figure 1A). Nevertheless, we speculated that
310 the beta power fluctuations likely differed in phase between the two groups, and we extracted the

311 phase of the beta power time series at 2 Hz (the stimulus presentation rate) from the frequency
312 transformation above (Figure 1C) for subsequent exploratory analyses. Note that the phase of
313 beta power time series refers to the peak/trough position of the fluctuations in the measured beta
314 power relative to the onsets of the stimuli. A Watson-Williams two-sample test showed that the
315 phase of the beta power time series differed significantly at right auditory cortex ($F(1,24) =$
316 12.90 , $p = .002$), but not at left auditory cortex, although there was a trend for a difference
317 ($F(1,24) = 3.51$, $p = .073$). The interaction between groups and left/right auditory cortex (taking
318 the circular difference between hemispheres within each participant, and then performing a
319 between-subject Watson-Williams test) was not significant ($F(1,24) = 1.57$, $p = .222$).

320 To investigate whether this significant right auditory cortex phase difference of beta
321 power fluctuation between groups was specific to 2 Hz, we further performed the same analyses
322 at 1 and 3 Hz in the right auditory cortex. At 3 Hz, there was no significant difference between
323 groups, $F(1,24) = 0.88$, $p = .356$. Further, the group difference was larger at 2 Hz than at 3 Hz
324 (taking the circular difference between frequencies within each participant, and then performing
325 a between-subject Watson-Williams test), $F(1,24) = 9.47$, $p = .005$. Thus, the phase differences
326 between groups were markedly larger at 2 Hz than at 3 Hz. At 1 Hz, the group difference was not
327 significant, but there was a trend, $F(1,24) = 3.33$, $p = .081$. There was also a trend for larger
328 group difference at 2 Hz than at 1 Hz, $F(1,24) = 3.37$, $p = .079$. Together these results suggest
329 that the phase difference of beta band power fluctuation is likely specific to 2 Hz, the rate of tone
330 presentation in the stimulus.

331

332 *Tapping production task.*

333 The two participant groups differed in neither synchronization consistency (vector length;
334 $t(23) = -0.10, p = .93$) nor synchronization accuracy (vector angle; Watson-Williams two-sample
335 test: $F(1,23) = 0.00, p = .99$). Both control and dyslexic participants performed well on the
336 tapping task, reaching synchronization consistency (vector length) close to one (controls: $.95$
337 $\pm .05$; dyslexics: $.95 \pm .04$) and synchronization accuracy (vector angle) suggesting weak
338 anticipation of the next tone (controls: $-11 \text{ ms} \pm 13$; dyslexics: $-15 \text{ ms} \pm 39$).

339

340 **Discussion**

341 The results of the current study revealed that the phase of beta power fluctuation was
342 different between adult university students with dyslexia and typical controls while listening to
343 an isochronous tone sequence. To the best of our knowledge, this is the first study reporting
344 atypical beta power entrainment in dyslexia.

345 The atypical beta power fluctuation in dyslexia might reflect deficits in tracking and/or
346 perceiving auditory rhythms. Previous studies on typical healthy participants showed that the
347 fluctuation of beta power reflects entrainment to the rhythmic regularity of an auditory sequence.
348 Specifically, the peaks of the beta power align to the onset of the tones, and are associated with
349 rhythm tracking and auditory perception and prediction (Chang et al., 2018, 2019; Cirelli et al.,
350 2014; Fujioka et al., 2009, 2012, 2015; Snyder and Large, 2005; Iversen et al., 2009). Our neural
351 findings are consistent with previous studies showing that individuals with dyslexia have deficits
352 in perceiving the rhythmic modulation of nonverbal auditory streams and speech (Goswami et
353 al., 2002; Goswami, 2011, 2015, 2019; Megnin-Viggars and Goswami, 2013). Nevertheless, it is
354 important to note that we cannot eliminate all explanations based on factors beyond entrainment,

355 such as, for example, that the participants in the Dyslexic group were more distracted by the
356 visual movie, leading to less attention to the auditory stimuli.

357 It was unexpected that the frequency spectrum of beta power fluctuation (Figure 1B) did
358 not show an obvious peak the at stimulus presentation rate (2 Hz). To the best of our knowledge,
359 our study is the first one reporting the spectrum of beta power fluctuation, while most previous
360 studies only reported its time-domain features. The lack of an obvious spectral peak could simply
361 be due to a smaller signal-to-noise ratio in the current study, as the number of trials was smaller
362 and the EEG recording time was shorter than in previous studies (e.g., Fujioka et al., 2012). It is
363 also possible that the power fluctuation was not perfectly periodic; the moment-to-moment
364 fluctuation rate might have drifted around 2 Hz on individual trials, and thus the 2 Hz peak was
365 not obvious in the averaged spectrum with traditional Fourier-based time-frequency
366 transformation approaches, which assume the signals to be stable over time. Future studies using
367 more advanced cycle-by-cycle analysis approaches (e.g., Cole and Voytek, 2019) are needed to
368 investigate the dynamic beta oscillatory activities.

369 There are a few studies reporting an association between beta oscillations and dyslexia. A
370 previous study reported that auditory steady-state response synchronization is reduced in the beta
371 frequency range in dyslexia, and that this response is associated with literacy skills (Van Hirtum
372 et al., 2019). Differences in overall beta power at occipital channels between individuals with
373 and without dyslexia have also been found during listening to noise-vocoded speech (Power et
374 al., 2016). An atypical hemispheric asymmetry of beta power in response to linguistic tasks has
375 also been associated with reading skill or processing phonological information in dyslexia (e.g.,
376 Penolazzi et al., 2010; Spironelli et al., 2008). The present study extends these studies by

377 indicating that the beta oscillatory activity in response to a simple, rhythmic (isochronous) sound
378 sequence is also atypical in dyslexia.

379 Atypical beta power fluctuation has also been observed in other disorders featuring
380 deficits in perceiving or tracking auditory rhythm. For example, Parkinson's patients are known
381 to have deficits in tracking auditory rhythms (Grahn and Brett, 2009; Grahn, 2012), and the
382 phase of their beta power fluctuation while perceiving auditory or visual rhythms was opposite to
383 that of the controls (te Woerd et al., 2017, 2018). Also, children with stuttering have deficits in
384 perceiving auditory rhythm (Chang et al., 2016b; Falk et al., 2015; Wieland et al., 2015), and the
385 phase of their beta power fluctuation was also opposite to that of controls (Etchell et al., 2016).

386 Although previous studies investigating children with dyslexia showed deficits in their
387 ability to tap to a beat or perceive a beat (Muneaux et al., 2004, Thomson and Goswami, 2008),
388 in the present study, performance on a simple metronome tapping task did not differ between
389 adults with dyslexia and typical controls, and we failed to find any associations between atypical
390 beta power fluctuation and tapping production performance to the same isochronous sequence
391 (Figure S2). In addition to the relatively small sample size and thus potentially insufficient
392 statistical power, it is possible that (1) our task was too easy and thus not sensitive enough to
393 reflect a deficit in rhythm processing in dyslexia. Indeed, in another study, our participants with
394 dyslexia were worse than controls (Canette et al., 2020) on performing more complex tapping
395 task (e.g., tapping to the beat of musical excerpts). Furthermore, (2) individuals with dyslexia
396 might find other ways and use different neural mechanisms to compensate as they get older (cf.
397 Shaywitz et al., 2003; Law et al., 2015), making it challenging to directly associate beta
398 oscillation with rhythmic abilities. In particular, previous behavioral studies have revealed
399 greater deficits in tapping tasks for dyslexic adolescents than for dyslexic university students,

400 who performed as well as controls on some of the measures (Wolff et al., 1990; see also
401 Thomson et al., 2006). Furthermore, the observed variability of the dependent measures of the
402 participants with dyslexia in our study suggests that individuals might use different neural
403 mechanisms.

404 In additional analyses examining ERPs (presented in the *Supplementary Materials*),
405 another common approach to examining auditory neural signature of dyslexia, we found a group
406 difference in an early ERP component at the P1 latency at Fpz, and a marginal correlation
407 between this component and the phase of beta power fluctuation (Figure S1). A possible post hoc
408 explanation is that the atypical beta power fluctuation in dyslexia is associated with deficits in
409 early auditory processing, such as encoding rise time and duration (Bamiou et al., 2001;
410 Hämäläinen et al., 2013; Sharma et al., 2009; King et al., 2003). However, our study was not
411 designed to examine this possibility, so future studies are needed with a larger sample size to
412 investigate this possibility.

413 The current study did not investigate delta (1-3 Hz) oscillations or their cross-frequency
414 coupling with beta oscillations, despite previously reported associations between delta
415 oscillations and dyslexia. Both animal electrophysiology and human neuroimaging studies have
416 shown that the delta oscillation phase time-locks and entrains to external rhythmic sensory input
417 (see Haegens and Zion Golumbic, 2018 for a review) and it has been reported that atypical delta
418 phase entrainment is associated with deficits of rhythm perception and tracking among
419 individuals with dyslexia (Colling et al., 2017; Di Liberto et al., 2018; Molinaro et al., 2016;
420 Power et al., 2013, 2016). However, recent studies have shown that it is challenging to reliably
421 quantify delta phase entrainment because the frequency-domain signature of ERP activity
422 typically overlaps with low-frequency oscillations in Fourier-based analysis (Doelling et al.,

423 2019; Haegens and Zion Golumbic, 2018). For this reason, we have left the question of how
424 delta and beta oscillations are related in dyslexia to future studies with materials and designs
425 more appropriate for addressing this question. Note that the induced beta oscillations measured
426 in the current study are unlikely to be confounded with ERPs because (1) the mean spectrum of
427 the ERP showed that the power above 15 Hz was neglectable (Figure S4), and (2) we removed
428 the phase-locked evoked activity from the induced activity in the beta band prior to conducting
429 our analyses.

430 Understanding atypical beta power entrainment could potentially benefit individuals with
431 dyslexia. Studies have shown that rhythmic auditory or musical training can improve the
432 phonological awareness and reading skills in children with dyslexia, including randomized
433 control trials (e.g., Cogo-Moreira et al., 2013; Flaunacco et al., 2015; Habib et al., 2016;
434 Thomson et al., 2013). The efficacy of longer-term musical rhythm training in language
435 remediation is likely related to the importance of rhythm for decoding the speech stream
436 (Flaunacco et al., 2015; Kotz and Schwartz, 2010; Overy, 2000; Schön and Tillmann, 2015).
437 In typically-developing children and in children with language disorders, presenting a rhythmic
438 prime has been shown to immediately improve syntactic processing over the short term (Bedoin
439 et al., 2016; Chern et al., 2018; Przybylski et al., 2013). Future studies are needed to investigate
440 whether beta power entrainment is an underlying neural mechanism of these effects, and whether
441 individual differences in beta power entrainment could predict the potential benefit of auditory
442 rhythmic habilitation programs.

443

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454

455 **Conflict of Interest Statement**

456 None.

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459

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653

654 **Figure Legend**

655

656 **Figure 1. The beta (15-25 Hz) power at bilateral auditory cortices.** (A) The beta power time
657 series are presented as the mean \pm standard error across typical (control) and dyslexic
658 participants. (B) The spectra of beta power fluctuation (note that this is not the spectra of the raw
659 EEG waveform). (C) The phases of beta power time series at 2 Hz. Each blue arrow represents
660 the phase angle of beta power for a single participant; the phase angles and lengths of the red
661 arrows represent the group-averaged angle and consistency of the angle distribution,
662 respectively. The phase angles differed significantly between groups at the right auditory cortex.
663 (p: p-value; a.u.: arbitrary unit)

664

